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Original Research

To use diffusion tensor imaging for precise mapping of white matter pathways in relation to brain cancers

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ABSTRACT:

Aim: To use diffusion tensor imaging for precise mapping of white matter pathways in relation to brain cancers. **Materials and methods:** This cross-sectional, prospective, hospital-based studywas conducted in the Department of Radiodiagnosis. A total of 50 patients with brain tumours were evaluated. Informed consent was received from all patients or the participant's parents or legal guardian and the studies were approved by the hospital's Research Ethics Committee. They underwent conventional MRI supplanted by diffusion tensor imaging in Philips Achieva 3T scanner. DTI was performed using dual spin echo, a single shot, a pulsed gradient and an echo-planar imaging (EPI) sequences, single-shot spin echo, echo-planar imaging (EPI) and parallel imaging techniques to achieve motion-free and higher signal-to-noise ratio (SNR) DTI. **Results:** We found that mean FA value for displaced WMFT was 0.462 with standard deviation of 0.049 while mean ADC value was 0.721 with standard deviation of 0.112. In case of edematousfibers, we found that mean FA value was 0.414 with standard deviation of 0.044 while mean ADC value was 1.339 with standard deviation of 0.118. Infiltrated fibres showed mean FA value of 0.382 with standard deviation of 0.045. Mean ADC value for infiltrated fibers was 1.026 with standard deviation of 0.088. In case of disrupted fibers, we observed significant drop in FA value compared to normal contralateral side. Mean FA value for disrupted fibers was 0.290 with standard deviation of 0.055. However, ADC values for disrupted fibers were not strikingly different from that for infiltrated fibres. Mean ADC value for disrupted fibers was 1.025 with standard deviation of 0.085. **Conclusion:** The FA and ADC values of white matter fibre tracts affected by tumour and peritumoural oedema can be of assistance when evaluating the malignant potential, extent and operability of the tumour, even though the FA and ADC values cannot be associated with the specific histology of the tumour.

Keywords: Diffusion tensor imaging, White matter, Brain malignancies

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INTRODUCTION

Diffusion Tensor Imaging (DTI) is a cutting-edge neuroimaging technique that has revolutionized the study of white matter in the brain. By leveraging the principles of diffusion-weighted imaging (DWI), DTI provides detailed insights into the microstructural organization of white matter tracts, offering unprecedented opportunities for mapping the complex neural pathways that traverse the brain. This technique has become particularly valuable in the context of brain malignancies, where accurate delineation of white matter tracts is crucial for both diagnosis and surgical planning.[1,2] White matter tracts are the conduits through which neural signals are transmitted across different regions of the brain. These tracts consist of bundles of myelinated axons that facilitate rapid communication between neurons, supporting essential functions such as motor control, sensory perception, and cognitive processes. The integrity and organization of these tracts are vital for normal brain function, and any disruption—whether due to disease, trauma, or surgical intervention—can lead to significant neurological deficits.[3]Brain malignancies, such as gliomas, meningiomas, and metastatic tumors, often infiltrate or compress adjacent white matter tracts, leading to alterations in neural connectivity and function. The relationship between brain tumors and white matter tracts is complex; tumors can displace, infiltrate, or even destroy these pathways, depending on their location, size, and aggressiveness. Consequently, accurately mapping the white matter tracts in relation to brain malignancies is critical for understanding the impact of the tumor on brain function and for guiding

surgical interventions that aim to remove the tumor while preserving as much neurological function as possible.[4] DTI works by measuring the diffusion of water molecules in brain tissue. In white matter, water diffusion is highly directional due to the organized structure of the myelinated fibers, which restricts the movement of water molecules primarily along the length of the axons. This directional diffusion, known as anisotropy, is the basis for generating the images and data that reveal the orientation and integrity of white matter tracts. DTI provides several key metrics, including fractional anisotropy (FA), mean diffusivity (MD), and eigenvectors, which together allow for the visualization and quantification of white matter tracts.[5]

One of the primary applications of DTI in the context of brain malignancies is in preoperative planning. Neurosurgeons rely on precise mapping of white matter tracts to plan surgical approaches that minimize damage to critical pathways, thereby reducing the risk of postoperative deficits. For example, in patients with tumors located near the corticospinal tract, which is responsible for motor function, DTI can help delineate the exact position of this tract relative to the tumor. This information enables surgeons to plan a resection strategy that maximizes tumor removal while preserving motor function. Similarly, DTI can be used to map language pathways, such as the arcuate fasciculus, in patients with tumors near language centers, helping to avoid postoperative language impairments.[6] Beyond surgical planning, DTI also plays a role in the diagnosis and characterization of brain malignancies. The pattern of white matter disruption observed on DTI can provide insights into the nature of the tumor. For instance, high-grade gliomas are often associated with significant infiltration of white matter tracts, leading to a reduction in FA values and altered tractography. In contrast, benign tumors, such as meningiomas, may displace white matter tracts without infiltrating them, resulting in different patterns of diffusion abnormalities. By analyzing these patterns, clinicians can gain a better understanding of tumorbehavior and its impact on brain function, which can inform treatment decisions.[7] Furthermore, DTI has applications in monitoring the effects of treatment. After surgical resection, radiation therapy, or chemotherapy, DTI can be used to assess changes in white matter integrity and to detect early signs of recurrence or treatment-related damage. This is particularly important in the management of brain tumors, where early detection of recurrence can significantly impact patient outcomes.Despite its advantages, DTI is not without limitations. The resolution of DTI is limited compared to other imaging modalities, and its accuracy can be affected by factors such as patient movement, the presence of edema, and the complexity of crossing fibers. Additionally, while DTI provides valuable information about the structure of white matter tracts, it does not directly measure function, necessitating the integration of DTI with other modalities, such as functional MRI (fMRI), for a more comprehensive assessment of brain function in relation to tumors.[8]

MATERIALS AND METHODS

This cross-sectional, prospective, hospital-based studywas conducted in the Department of Radiodiagnosis. A total of 50 patients with brain tumours were evaluated. Informed consent was received from all patients or the participant's parents or legal guardian and the studies were approved by the hospital's Research Ethics Committee. They underwent conventional MRI supplanted by diffusion tensor imaging in Philips Achieva 3T scanner. DTI was performed using dual spin echo, a single shot, a pulsed gradient and an echo-planar imaging (EPI) sequences, single-shot spin echo, echo-planar imaging (EPI) and parallel imaging techniques to achieve motion-free and higher signal-to-noise ratio (SNR) DTI. The total imaging time for DTI and FT was 7–9 minutes according to the section numbers, which was added to the routine MR imaging examinations. (TR-6.6s, TE – 70ms, voxel size 2 x 2 x 2mm, FOV – 224x224x120mm, B value 800s / mm2, SAR mode-high). Anisotropy was calculated by using orientation-independent fractional anisotropy (FA), and diffusion-tensor MR imaging– based color maps were created from the FA values and the three vector elements. The vector maps were assigned to red (x element, left-right), green (y, anterior-posterior), and blue (z, superior- inferior) with a proportional intensity scale according to the FA. The threshold values for the termination of the fiber tracking were less than 0.2 for FA and greater than 25° for the trajectory angles between the ellipsoids. For tracking of the white matter fibers, the region of interest (ROI) method was applied. We placed the single or multiple ROIs on the color maps. The plane of the ROI was varied according to the running direction of the white matter fibers (e.g., corticospinal tract on the axial views, corpus callosum on the sagittal views).

RESULTS

Among 50 patients in our study 33 were male and 17 female patients. Youngest among these was 3 years old male and oldest patient was 77 years old female. Mean age was 41.1 year. These patients were classified into age groups of 0- 15 years, 16 -30 years, 31- 45 years, 46 – 60years and > 60 years of age. In the first group that is 0-15 years, we observed 8 male patients and 4 female patients. In 16 – 30 years age group, we observed 6 male patients and 1 female patient. In 31- 45 years age group, we observed 3 male and female patients. In 46- 60 years age group, we observed 11 male patients and 1 female patient. In >60 year age group, we observed 4 male patients and 8 female patients. We included handedness of patient locate dominant hemisphere, as it is the simplest way of doing so. 43 patients were right handed and 7

patients were left handed. Among these, 29 male and 14 female patients were right handed, while 4 male and 3 female patients were left handed. Among 50 patients in our study, 39 had lesion in supratentorial location with 25 male and 14 female patients in this category. Infratentorial lesion was seen in 8 male and 3 female patients. Space occupying lesions are described according to their location and broader morphological characteristics on conventional MRI.We examined all the patients for neurological deficit and documented affection of motor and sensory function, speech and vision in them. After reaching the radiological diagnosis of lesion (evaluated by senior consultant radiologists), we collaborated with neurosurgical team to chalk out best possible surgical approach and management for the space occupying lesion. Later we evaluated these patients using diffusion tensor imaging and fiber tractography complimentary to the conventional MRI. We evaluated relevant white matter fiber tracts (WMFT) in supra- and infratentorial compartments and documented their FA and ADC values. We classified them into four classes i. e. displaced, edematous, infiltrated and disrupted; according to altered FA and ADC values and whether they lie in normal or abnormal MRI signal intensity area on conventional images. We also considered anatomical location and orientation of fiber tracts, their density or clustering compared to contralateral side. Our imaging findings were later correlated with intraoperative findings. We found that mean FA value for displaced WMFT was 0.462 with standard deviation of 0.049 while mean ADC value was 0.721 with standard deviation of 0.112. In case of edematousfibers, we found that mean FA value was 0.414 with standard deviation of 0.044 while mean ADC value was 1.339 with standard deviation of 0.118. Infiltrated fibres showed mean FA value of 0.382 with standard deviation of 0.045. Mean ADC value for infiltrated fibers was 1.026 with standard deviation of 0.088. In case of disrupted fibers, we observed significant drop in FA value compared to normal contralateral side. Mean FA value for disrupted fibers was 0.290 with standard deviation of 0.055. However, ADC values for disrupted fibers were not strikingly different from that for infiltrated fibres. Mean ADC value for disrupted fibers was 1.025 with standard deviation of 0.085.

Table 1: Demographic and Age Distribution of Patients

Age Group (Years)	Number of Male Patients	Number of Female Patients	Total Patients
0-15	8	4	12
16-30	6	1	7
31-45	3	3	6
46-60	11	1	12
>60	4	8	12
Total	**33**	**17**	**50**

Table 2: Handedness of Patients

Handedness	Number of Male Patients	Number of Female Patients	Total Patients
Right-handed	29	14	43
Left-handed	4	3	7
Total	**33**	**17**	**50**

Table 3: Lesion Location Distribution

Lesion Location	Number of Male Patients	Number of Female Patients	Total Patients
Supratentorial	25	14	39
Infratentorial	8	3	11
Total	**33**	**17**	**50**

Table 4: Classification of White Matter Fiber Tracts (WMFT) by FA and ADC Values

WMFT Class	Mean FA Value	Standard Deviation (FA)	Mean ADC Value	Standard Deviation (ADC)
Displaced	0.462	0.049	0.721	0.112
Edematous	0.414	0.044	1.339	0.118
Infiltrated	0.382	0.045	1.026	0.088
Disrupted	0.290	0.055	1.025	0.085

DISCUSSION

In our study we observed mainly four patterns of involvement white matter fibre tracts. Pattern 1 consisted of normal or only slightly decreased FA with abnormal location and/or direction resulting from bulk mass displacement. This is the most clinically useful pattern in preoperative planning because it confirms the presence of an intact peri tumoral tract that can potentially be preserved during resection. Pattern 2 was substantially decreased FA with normal

location and direction (i.e, normal hues on directional colour maps). This is frequently observed pattern in regions of vasogenic edema, although the specificity of this pattern is not yet known especially in case of high-grade gliomas. Pattern 3 was substantially decreased FA with abnormal hues on directional color maps. This pattern is identified in a small number of infiltrating gliomas in which the bulk mass effect appeared to be insufficient to account for the abnormal hues on directional maps. It is speculated that infiltrating tumour disrupts the directional organization of fibre tracts to cause altered colour patterns on directional maps, but this phenomenon requires further study. Pattern 4 consisted of isotropic (or near isotropic) diffusion such that the tract cannot be identified on directional color maps. This pattern is observed when some portion of a tract is completely disrupted by tumor. Here FA values were significantly low. This pattern can be useful in preoperative planning in the sense that no special care need be taken during resection to preserve a tract that is shown by DTI to be destroyed. It should be noted that combinations of the above patterns may occur; for example, a combination of patterns 1 and 2 may be observed in a tract that is both displaced and edematous. These findings were in concordance with previous studies done by aoron field et al.[8], jellison et al.[9] and witwer et al.[10] In our study The FA values of displaced WMFT ranged between 0.413-0.511. The FA values of edematous WMFT ranged between 0.370-0.458. The FA values of infiltrated WMFT ranged between 0.337-0.427. The FA values of displaced WMFT ranged between 0.235-0.345. The ADC values (× 10-3 mm2/s) of displaced WM fibers ranged from 0.609 to 0.833. The ADC values (× 10-3 mm2/s) of edematous WM fibers ranged from 1.221 to 1.457. The ADC values (× 10-3 mm2/s) of infiltrated WM fibers ranged from 0.938 to 1.114. The ADC values (× 10-3 mm2/s) of disrupted WM fibers ranged from 0.940 to 1.110. Various studies like Sinha et al.[11] and Lu et al.[12] used measures of mean diffusivity and fractional anisotropy to differentiate normal white matter, edematous brain, and enhancing tumor margins. Anisotropy is reduced in cerebral lesions due to the loss of structural organization in studies by Wieshmann et al..[13] and Mascalchi et al.[14] In studies by Beppu et al. [15] and Price et al.[16] It seems that the abnormalities on DTI are more significant than those seen on T2-weighted images in high grade gliomas. Second, DTI may distinguish if the white matter fibers are displaced (Wieshmann et al..[17] and Gossl et al.[18]), infiltrated, or disrupted by the tumor (Witwer et al.[10]). Finally, the fiber-tracking technique (DTI-FT) that is able to identify and reconstruct the main white matter connections. This information is very useful for presurgical planning, delineating the spatial relationships of eloquent structures and tumors in order to preserve the functional pathways intraoperatively (Holodny et al.[19] Tummala et al[.20] Henry et al.[21]). Our study support these findings and we recommend routine DTI-FT evaluation of intracranial tumors affecting brainstem and eloquent brain cortex for optimal neurosurgical management and favourable outcome. Diffusion-tensor imaging documented deviation of fibers in normal-appearing white matter in relation to the anterior commissure – posterior commissure line when compared with contralateral side. DTI mapping brings complementary information that helps elucidating the complex relationships between the tumor and its surrounding cerebral tissue. Knowledge of direction of displacement assisted in preoperative planning by informing the surgeon of the tract's shifted location, thus allowing for adaptation of the surgical corridor to avoid destruction of the communicating white matter bundles. In one of our patient the tumor was approached from a temporal posterior direction, allowing for aggressive resection of the tumor while avoiding the anteriorly deviated motor fibers. This resulted in postoperative improvement of the patient's hemiparesis, presumably due to the elimination of pressure on the corticospinal tracts.

CONCLUSION

The FA and ADC values of white matter fibre tracts affected by tumour and peritumoural oedema can be of assistance when evaluating the malignant potential, extent and operability of the tumour, even though the FA and ADC values cannot be associated with the specific histology of the tumour.

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